Comparative Analysis of ECG Data Augmentation Methods in Arrhythmia Classification



Jonas Mindaugas Rimšelis, Povilas Treigys, Zigmantas Kestutis Juškevičius, Jolita Bernatavičienė

Institute of Data Science and Digital Technologies, Vilnius University

Introduction

An electrocardiogram (ECG) measures electrical signals from the heart to capture various cardiovascular conditions. Distinct patterns can be identified in ECG signals during the development of arrhythmias. The growing availability of single-lead Holter devices enables continuous cardiac monitoring and supports earlier arrhythmia detection using deep learning [1]. Since abnormal heartbeats occur rarely, even in patients diagnosed with arrhythmia, data used for training models are imbalanced, leading to poor generalization and robustness [2]. To circumvent this, data augmentation is utilized to mitigate label balancing issues. This study is split into two parts:

- Literature review of data augmentation techniques and preprocessing methods;
- Empirical study of Synthetic Minority Over-sampling Technique (SMOTE) and Denoising Diffusion Probabilistic Model (DDPM) models to improve the accuracy of arrhythmia beat classification.

MIT-BIH Arrhythmia Database

Table: Beat Counts of the MIT-BIH Arrhythmia Database by AAMI Class and DS1/DS2 split with adherence to AAMI labels and inter patient paradigm

AAMI Class	DS1 (Training Set) Beats	DS2 (Testing Set) Beats	Total Beats
N (Normal)	45,866	44,259	90,125
S (Supraventricular)	944	1,837	2,781
V (Ventricular)	3,788	3,221	7,009
F (Fusion)*	415	388	803
Q (Unclassified)*	8	7	15
Total	51,013	49,705	100,718

*Note: Q-class beats are **excluded** from training, while F beats from evaluation, allowing the analysis to focus on clinically relevant minority classes, particularly the S-class.

Literature Review

Table: Literature review results.

Ref.	Preprocessing	Segmentation	Augmentation	Classifier	Accuracy
[3]	Butterworth BP	Beat seg., convert to image	Auxiliary Clas- sifier GAN	LC-CNN	99.22%
[4]	Butterworth BP	Beat seg.	BC-GAN	MISEResNet- BiLSTM	99.93%
[5]	_	Beat seg., convert to image	Multimodality Data Matching- Based	Multimodality Feature Encoding, Fusing, Sof- max	98.83%
[6]	-	Beat seg.	TCGAN	Multi-scale Conv1d + Bi-LSTM	94.69%
[7]	Wavelet de- noising	5-10s seg.	Stretching, scaling, Gaus- sian noise	dual path CNN- BiLSTM	95.48%
[8]	Butterworth BP, zscore normalization	Beat seg.	K-means un- dersampling + SMOTE	MB-MHA- TCN	98.75%
[9]	Min-Max nor- malization	10s seg., norm., beat seg.	SMOTE, ADASYN	CNN	SMOTE: 94.75%, ADASYN: 95.78%
[10]	_	Beat seg.	TimeGAN, ECGAN, DDPM	t-SNE	TimeGAN: 79.2 ± 12.8, EC GAN: 93.8 ± 5.1 DDPM: 69.2 ± 18.6
[11]	-	Beat seg., convert to image	DCGAN, CGAN, WGAN-GP	2D-CNN	Normal class: 77.9%; Abnormal class: 93.1%

Classifier

2D-CNN-BiLSTM classifier was chosen for the classification task:

- Inputs: the raw beat segment, a QRS complex mask, and R-R interval features.
- A 3-layer 2D-CNN with a BiLSTM. Concurrently, R—R features are embedded from 3D to 16D.
- A 2-layer MLP is used for the class assignment.

Training process: 15 epochs with Focal Loss (No augmentation; DDPM weights: N–0.08, S–0.72, V–0.15, F–0.05; SMOTE weights: N–0.24, S–0.47, V–0.24, F–0.06). Because the F class received a very small effective weight, the model did not learn this class reliably; therefore, F-class performance is omitted from the results section.

Data augmentation methods

- **SMOTE** with k neighbors set to 3 was utilized to augment the beat-level segment vector with concatenated RR features.
- **DDPM** architecture consists of a 1D U-Net with skip connections and ResBlock1D. Generated signals were filtered to have at least 0.3 correlation with their original signal. Example of the generated signals:

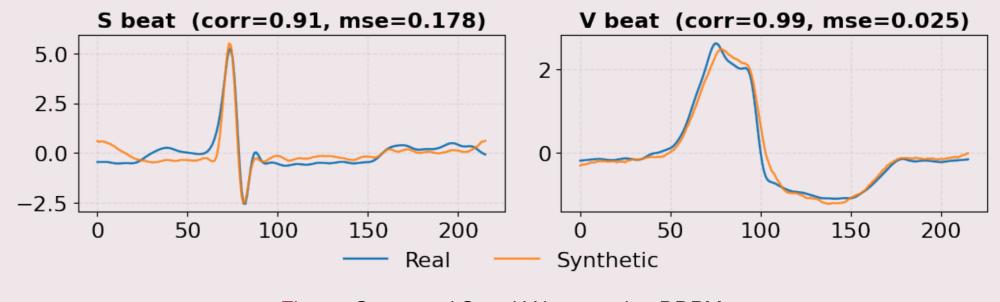


Figure: Generated S and V beats using DDPM

Insights

- **Preprocessing and segmentation:** Filtering and denoising steps are rarely used, but Butterworth bandpass filters followed by Z-score or Min-Max normalization coupled with beat-level segmentation are the standard.
- **Augmentation:** Generative Adversarial Networks (GANs) have replaced traditional methods (like SMOTE) as the most common approach for data augmentation.
- The highest accuracy of 99.83% was achieved using BC-GAN (which uses both BiL-STMs and CBAM modules) for data augmentation.
- An emerging trend of converting beats to images and augmenting data with an Auxiliary Classifier GAN resulted in an accuracy of 99.22%.

For further research, SMOTE was chosen as a baseline for augmentation and DDPM for its novelty in ECG signal augmentation and its capability to generate realistic waveforms.

Results

Conclusions and Future Work

Table: Classification performance per class using different augmentation methods.

Method	Class	Precision	Recall	F1-score	Overall Acc.
No augmentation (Z-score)	N	0.96	0.98	0.97	0.93
	S	0.28	0.33	0.30	
	V	0.92	0.77	0.84	
SMOTE (Min-Max)	N	0.95	0.80	0.86	0.77
	S	0.11	0.33	0.16	
	V	0.75	0.77	0.76	
DDPM (Z-score)	N	0.96	0.97	0.97	0.94
	S	0.40	0.31	0.35	
	V	0.85	0.92	0.88	

- Classifier trained on SMOTE-augmented data performed worse (Overall Acc. 77%)
 than the baseline classifier with no augmentation (Overall Acc. 93%).
 - The DDPM method increased S-beat precision by 12% and F1-score by 5% compared to the baseline method.
- Focal loss with stronger class weighting can partially alleviate class imbalance. Future work includes:
- Enhancing temporal feature extraction within the classifier architecture;
- Experimenting with GAN-based approaches for data augmentation;
- Incorporating longer ECG segments during training and augmentation to capture richer temporal dynamics.

Preprocessing Segmentation Data augmentation Classifier Normalization Testing data Figure: Overview of the ECG classification pipeline.

References

https://github.com/jonasmindaugasr/damms2025dataaugmentation